## CO-SEG: AN IMAGE SEGMENTATION FRAMEWORK AGAINST LABEL CORRUPTION

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## **ABSTRACT**

Supervised deep learning performance is heavily tied to the availability of high-quality labels for training. Neural networks can gradually overfit corrupted labels if directly trained on noisy datasets, leading to severe performance degradation at test time. In this paper, we propose a novel deep learning framework, namely Co-Seg, to collaboratively train segmentation networks on datasets which include low-quality noisy labels. Our approach first trains two networks simultaneously to sift through all samples and obtain a subset with reliable labels. Then, an efficient yet easily-implemented label correction strategy is applied to enrich the reliable subset. Finally, using the updated dataset, we retrain the segmentation network to finalize its parameters. Experiments in two noisy labels scenarios demonstrate that our proposed model can achieve results comparable to those obtained from fully supervised learning trained on the noise-free labels. In addition, our framework can be easily implemented in any segmentation algorithm to increase its robustness to noisy labels.

*Index Terms*— Deep Learning, Weakly Supervised Learning, Image Segmentation

# 1. INTRODUCTION

Recent years have witnessed an upsurge of interests in biomedical segmentation. Based on fully convolutional networks, U-Net [1] has been emerging as a classic model which concatenates multi-scale features from the downsampling layers and the upsampling layers. By stacking two U-Net architectures on top of each other, DoubleU-Net [2] is an improved version of U-Net aiming to achieve higher performance on specific tasks. CE-Net [3] modifies U-Net structure by adopting pretrained ResNet blocks in the feature encoding step to capture high-level spatial information. However, these fully supervised learning algorithms are vulnerable to label noise and their performance may be hugely degraded by noisy labels. Therefore, under noisy labels conditions, it is important to identify and selectively learn from a clean and

reliable subset of samples which mainly include data with clean labels, rather than learning from the whole sample set.

How to improve deep learning performance under noisy labels conditions has caught great attention [4, 5, 6, 7, 8, 9]. One direction is to estimate the mathematical model of a noise distribution [6, 7]. [7] proposes two procedures for loss correction based on noise transition matrix estimation. Another direction is to directly train on clean samples [8, 9]. Coteaching [8] trains two networks simultaneously to pick clean samples for each one. However, most current approaches focus on classification tasks, which cannot be applied to the segmentation where labels are spatially arranged in a dense manner. Finally, sample-based reweighting methods [9, 10] just ignore or assign small weights on noisy samples, which can lead to severe overfitting, especially for small datasets.

In this paper, we propose a novel deep learning framework for image segmentation, namely Co-Segmentation (Co-Seg), to handle noisy labels. Our framework integrates the idea of selective training and label correction. In particular, we propose a robust training network to collaboratively learn and select samples with reliable labels. Then a label correction scheme is proposed to enrich the reliable dataset and we retrain a new network on the updated dataset. Experimental results using Co-Seg on noisy labels show performance comparable to supervised learning on noise-free labels. In summary, this paper has the following contributions:

- (1) We develop an easily-implemented yet effective framework for image segmentation tasks with noisy labels. It can be easily applied to any deep learning segmentation model to increase learning ability under noisy labels conditions.
- (2) We demonstrate that, in multiple noise settings, our model achieves comparable results to supervised training on noise-free labels.

# 2. METHODOLOGY

Our proposed framework consists of 3 modules: (1) robust training module against noisy labels, (2) label correction module, and (3) retraining module, as shown in Fig. 1. The

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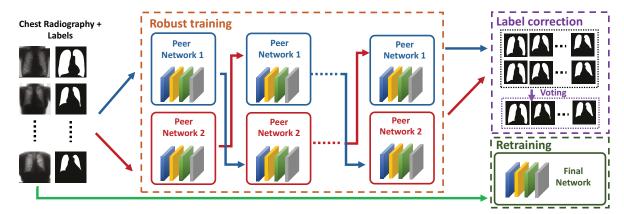


Fig. 1. Algorithm flow of Co-Seg framework.

robust learning module trains two segmentation networks simultaneously and selects clean samples for their peer networks. Then, the label correction module employs a voting strategy to correct unreliable labels from the noisy samples measured by corruption scores. Lastly, a single segmentation network is trained on the updated dataset to finalize network parameters for future segmentation tasks.

# 2.1. Robust training against noisy labels

Robust training against noisy labels is very challenging due to memorization effects of deep learning models. Directly training on noisy labels, the networks can gradually overfit noisy samples. Inspired by [8], our robust training module collaboratively trains two networks (peer network 1 & 2) for clean sample selection. Each network picks up a small proportion of high-quality samples in every mini-batch based on ranked corruption scores. Then, such high-quality samples will be fed to its peer network for back propagation. Given a sample, the corruption score  $S_{\rm c}$  is:

$$S_c = -\sum_{x \in Q} \sum_{l=1}^{L} g_l(x) \log(p_l(x))$$
 (1)

where L is the number of classes,  $p_l(x)$  is the estimated probability of class l at pixel position  $x \in \Omega$  with  $\Omega$  the image domain and  $g_l(x)$  is the label of the ground truth. The corruption score measures the reliability of the sample. Samples with smaller corruption scores are more likely to be clean. The proportion of samples selected from the corruption score ranking is controlled by  $\alpha$ , which is related to the noise level of the labels.

The loss function of each segmentation network is a combination of a cross entropy loss  $L_{CE}$ , a Dice loss  $L_{Dice}$ , and a  $L_2$ -regularization term on the parameters  $W_f$  of the network:

$$L_{total} = L_{CE} + \lambda_1 L_{Dice} + \lambda_2 ||W_f||_2^2$$
 (2)

$$L_{Dice} = 1 - \frac{1}{L} \sum_{l=1}^{L} \frac{2 \sum_{x \in \Omega} (p_l(x)g_l(x))}{\sum_{x \in \Omega} (p_l(x))^2 + \sum_{x \in \Omega} (g_l(x))^2}$$
(3)

where  $\lambda_1$ ,  $\lambda_2$  are tuned parameters. Here, the Dice loss  $L_{Dice}$  is used to capture spatial and structural coherence in the segmentation tasks.

#### 2.2. Label correction

We propose to correct noisy labels in biomedical segmentation, rather than ignore or downweight them for two reasons. First, maintaining data size is essential. Training on small-size samples may easily lead to severe overfitting. This is particularly important in biomedical applications where reliable labels at expert level are limited. Second, some noisy samples contain pixels with accurate spatial annotations, which could benefit segmentation. This differs from an image-level classification task where clean and noisy labels are disjoint.

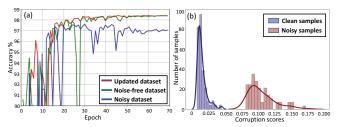
In the label correction module, labels in the training set are corrected based on the voting results from the two collaboratively trained networks obtained from the robust training module. First, we differentiate the noisy samples and the clean samples according to their corruption scores ranking. For each pixel in the noisy samples, we correct their labels if the prediction results from the two networks are the same but different from the input labels. Our updated dataset consists of clean samples with original labels and noisy samples with corrected labels. This process enriches the clean dataset with noise-corrected samples.

## 2.3. Retraining

Based on the updated dataset, we retrain a final segmentation network, which shares the same network structure as one of the peer networks. Similarly, the retraining uses loss function defined in Eq. 2. Then, this network will be used for final predictions.

# 3. EXPERIMENTS

We evaluated segmentation performance in two noisy settings, including both real-world labeling noise from an inex-



**Fig. 2**. Benchmark U-Net training behavior with 0.5 noise level and Co-Seg corruption scores. (a) Accuracy curves over training epochs under Type I noise. (b) Corruption scores under Type II noise: values and probability density functions from the whole training set.

perienced annotator and synthetic noise.

**Datatsets.** Our evaluation is based on chest X-rays from the Japanese Society of Radiological Technology (JSRT) dataset [11]. This dataset consists of 247 posterior-anterior (PA) chest radiographs. Ground-truth lung masks were obtained from the annotation of Radiographs (SCR) database [12] at expert level. Following previous work in [13, 14], we resize all images into  $256 \times 256$  pixels and split the training and testing sets by ID number: the training set contains 124 images with odd ID number and the testing set contains 123 images with even ID.

Label corruption scenarios. We conducted experiments using two scenarios of label corruption. (1) Synthetic boundary (Type I) noise. Manual segmentation variability usually occurs around tissue boundaries due to spatial uncertainty of contrast transition between different tissue types. Following [9], we generated boundary noise by randomly eroding or dilating tissue boundaries by  $n_i$  pixels with  $1 \le n_i \le 8$  in each direction; (2) Inexperienced annotation (Type II) noise. Human annotators tend to have a systematic bias toward over and under segmented tissue boundaries. To mimic this real-world noise scenario, an inexperienced annotator who was blind to the algorithm and ground truth, manually labeled the data and generated biased labels.

**Experimental setup.** As a demonstration of the framework, we choose the classic U-Net [1] as the network architecture to evaluate noise robustness performance and we adopt the same U-Net architecture and hyper-parameters for all segmentation networks in the robust training module (peer network 1 and 2 in Fig. 1) and retraining module (final network). We also use the performance of a single U-Net segmentation network with the same architecture trained on noise-free labels as a baseline for comparison. All networks are randomly initialized for fair comparison. The segmentation performance is evaluated by both accuracy (ACC) and Dice coefficient (DIC) in comparison with ground truth. The corrupted training sets are generated by replacing a proportion of clean labels with noisy labels. The noise level (NoL)is defined as the proportion of noisy labels in the training set. Following previous research [8, 9], we assume NoL is a known parameter and set  $\alpha = 1 - NoL$ .

**Table 1**. Evaluation metrics on lung segmentation with different label noise types (Type I and II explained in the text) and noise levels expressed as the proportion of noisy samples.

Network	Noise	Metrics	Noise level for Type I and II				
			0.1	0.2	0.3	0.4	0.5
Co-Seg	Type I	ACC	0.978	0.975	0.978	0.978	0.980
		DIC	0.975	0.973	0.975	0.974	0.976
	Type II	ACC	0.981	0.980	0.980	0.980	0.978
		DIC	0.974	0.974	0.975	0.975	0.973
U-Net	Noise Free	ACC			0.981		
		DIC			0.976		

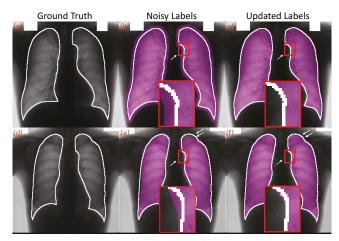
**Results.** Table 1 reports evaluation metrics for lung segmentation on the JSRT dataset with different label noise types and noise levels, together with the baseline experiment on noise-free labels using U-Net. The results obtained by our model are comparable with the baseline noise-free U-Net training. Differences are all below 0.6% in both DIC and ACC. Small variations among noise levels are likely caused by model stochasticity. Those results demonstrate that our Co-Seg model can provide robust results under noise levels up to 0.5 with performance similar to learning using noise-free labels.

We further visualize experimental results to show the effectiveness of the Co-Seg model. Fig. 2(a) compares the training accuracy curves (background and lung segmentation) from the benchmark U-Net trained using the updated labels, noise-free labels and the noisy labels over training epochs. The accuracy curve for the noisy labels (blue) decreases after 30 epochs indicating that the network is gradually overfitting the noisy samples. Meanwhile, the accuracy curve for the updated labels (red) is flat and smooth, showing consistency of training quality similar to the curve for the noisefree labels (green). Fig. 2(b) shows the corruption scores and their probability density functions for the entire training set with 0.5 noise level under Type II noise. The blue/red curves are the probability density functions fitted on the clean/noisy samples. The two probability density functions have (almost) disjoint supports, indicating that corruption scores effectively separate noisy and clean samples.

Figure 3 shows the effect of our label correction module in the two noise scenarios. In Fig. 3 (top row), the Type I noisy labels are well corrected. In Fig. 3 (bottom row), the Type II noisy labels are all well corrected at boundary locations marked by a single arrow. In addition, Co-Seg also fills in the large region of missing pixels marked by a double arrow.

# 4. CONCLUSIONS

In this paper, we develop a novel collaborative training framework, Co-Seg, to improve segmentation robustness against noisy labels. The robust training module uses two networks to learn representative features from samples detected as being reliable in a dataset with noisy labels. The label correction module employs a voting mechanism to trim the reliable set



**Fig. 3**. Label correction results with 0.5 noise level for Type I (top row) and Type II (bottom row) noise types. Ground-truth segmentation lung boundaries are shown in white while the noisy/updated labels are marked in pink.

prior to final retraining. Experimental results on both synthetic and real-world noisy labels scenarios show that our Co-Seg model is robust to label corruption and achieves comparable results with those trained with noise-free labels. Importantly, our training scheme is generic and can be easily applied to other deep learning models to increase labeling noise immunity. Future work will focus on extensive validation on more medical segmentation tasks, evaluation of potential bias of the label correction module toward selecting high-quality images and on the usefulness of applying more than two networks in the collaborative training.

Compliance with Ethical Standards: This research study was conducted retrospectively using human subject data made available in open access by the Japanese Society of Radiological Technology. Ethical approval was not required as confirmed by the license attached with the open access data.

**Acknowledgments:** The study was funded in part by the National Institute of Health (4DP2HL127776-02, CPH, subaward of UL1TR003096, YG), National Science Foundation (CRII-1948540, YG).

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